

The background of the slide is a dense field of red blood cells, rendered in a realistic, slightly glossy red color. The cells are packed closely together, filling the entire frame.

# Oxygen diffusion water, alkanes, and lipid bilayers

ACS Meeting New Orleans - April 10, 2013

An Ghysels

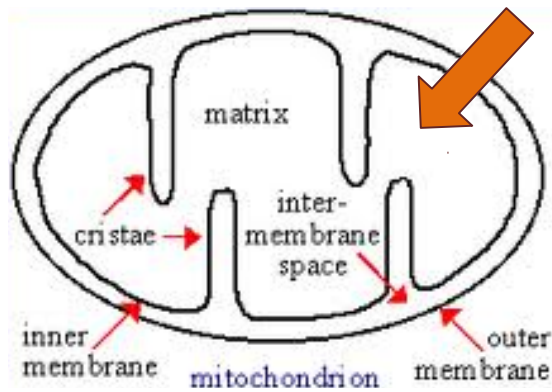
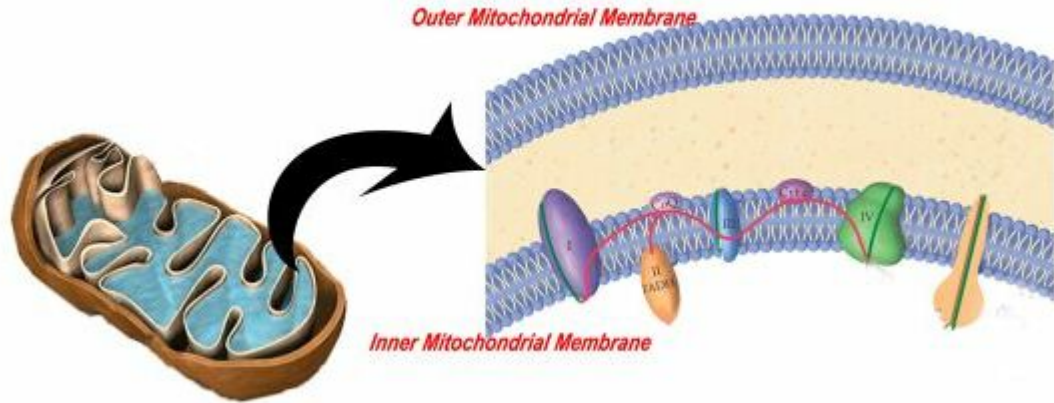
Ghent University

Center for Molecular Modeling

# Oxygen transport to the “fuel cells” of living organisms

Oxygen is consumed in the mitochondria.

**How does the very last step of the transport occur?**



Mitochondria have double membranes: inner and outer.

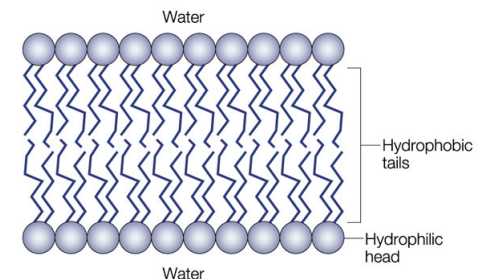
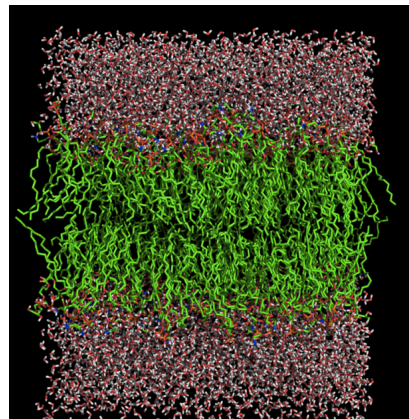
Inner membrane is a phospholipid bilayer

– curved (large surface)

– contains cardiolipin

–  $O_2$  has to diffuse through (or uses oxygen pumps)

We study this last step with molecular simulations



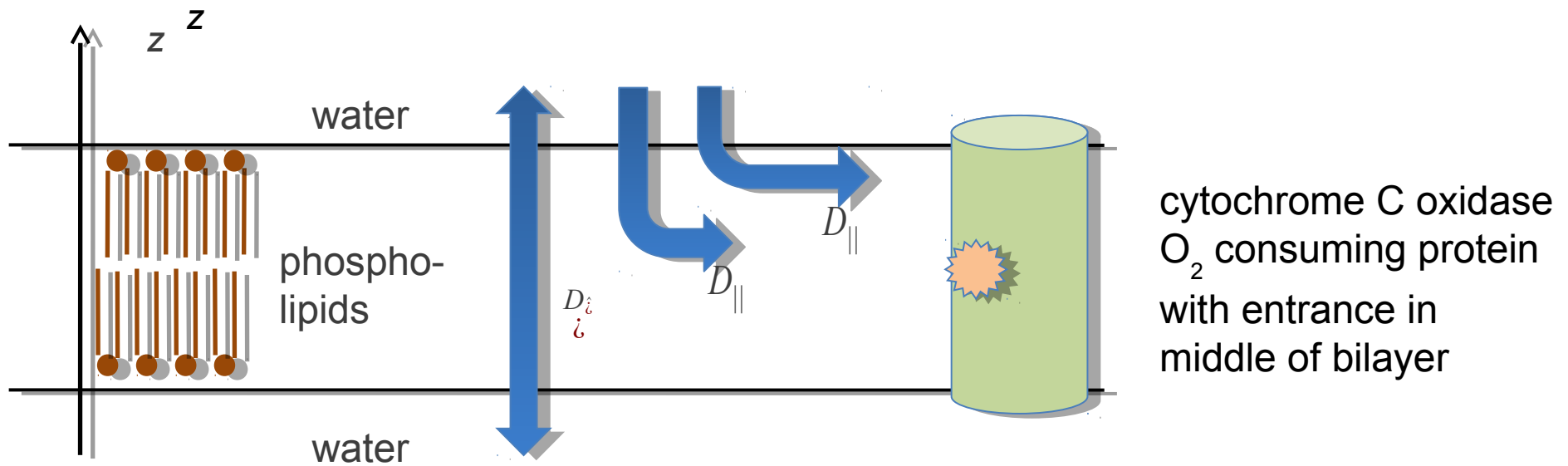
# O<sub>2</sub> transport through mitochondrial membranes

Where is O<sub>2</sub> motion slow, where fast?

Is there a build-up of O<sub>2</sub>?

Has cardiolipin an effect?

Optimal route to the middle of the layer?



=> needs a position-dependent description

**Key assumption:** O<sub>2</sub> behavior is approximately diffusive.

i.e. the time scale is large enough that the motion of O<sub>2</sub> seems random,

i.e. O<sub>2</sub> loses its 'memory' quickly,

## Position dependent diffusion 'constant'

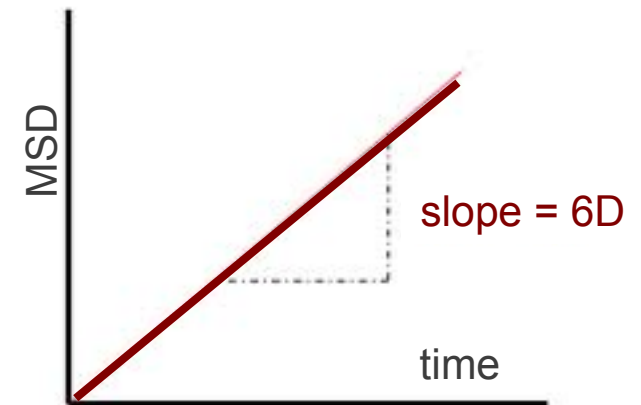
Difficult, because a lipid bilayer is inhomogeneous and anisotropic.

### Standard method to measure $D$

In a *homogeneous* and *isotropic* medium, mean square distance (MSD) grows linearly with time.

$$\text{MSD} = \langle \Delta r^2(t) \rangle = 6Dt \quad \text{when } t \rightarrow \infty$$

$$\frac{\partial p(\bar{r}, t)}{\partial t} = D \nabla^2 p(\bar{r}, t)$$



### In the lipid bilayer

- $D$  is a **tensor**,
- $D$  is **position-dependent**, and
- oxygen feels a position-dependent **mean field potential  $F$** .

$$\frac{\partial p(\bar{r}, t)}{\partial t} = \nabla \cdot \left[ \bar{\bar{D}}(\bar{r}) e^{-\beta F(\bar{r})} \nabla \left( e^{\beta F(\bar{r})} p(\bar{r}, t) \right) \right]$$

Smoluchowski equation

$p(\bar{r}, t)$  is the local oxygen concentration

## Outline – Simulating oxygen diffusion through membranes

1. Diffusion in inhomogeneous and anisotropic media
2. Five test systems:
  - pure water, pure hexadecane, hexadecane layer
  - simple POPC bilayer
  - model for inner mitochondrial membrane (MITO)
3. Deriving diffusion profiles from statistics
4. Free energy profiles and diffusion profiles

# Five studied systems

## 3 test systems for validation

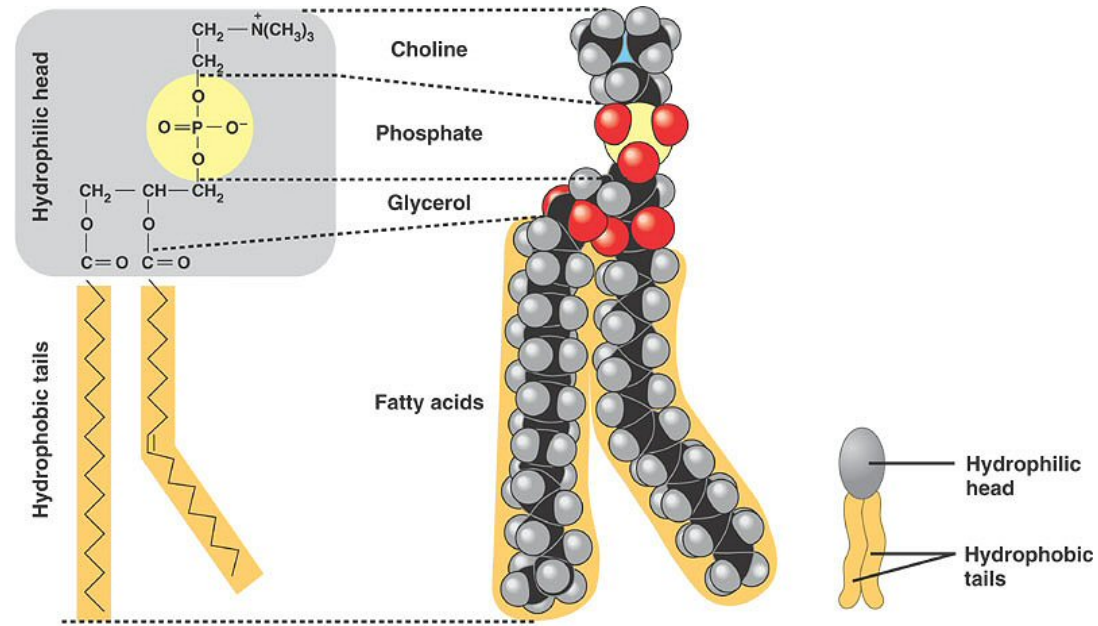
pure water

pure hexadecane

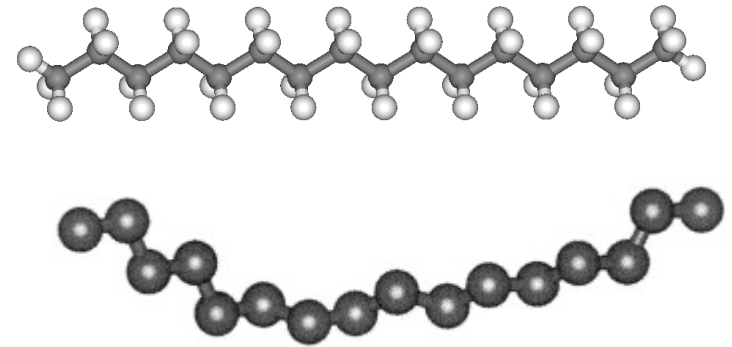
hexadecane layer  
in water

simple **POPC** bilayer  
containing only one lipid type

inner mitochondrial membrane: **MITO**  
modeled as bilayer with four lipid types



model: (C16) hexadecane C<sub>16</sub>H<sub>34</sub>  
is less inhomogeneous,  
resembles tails of lipids



# Five studied systems

3 test systems for validation

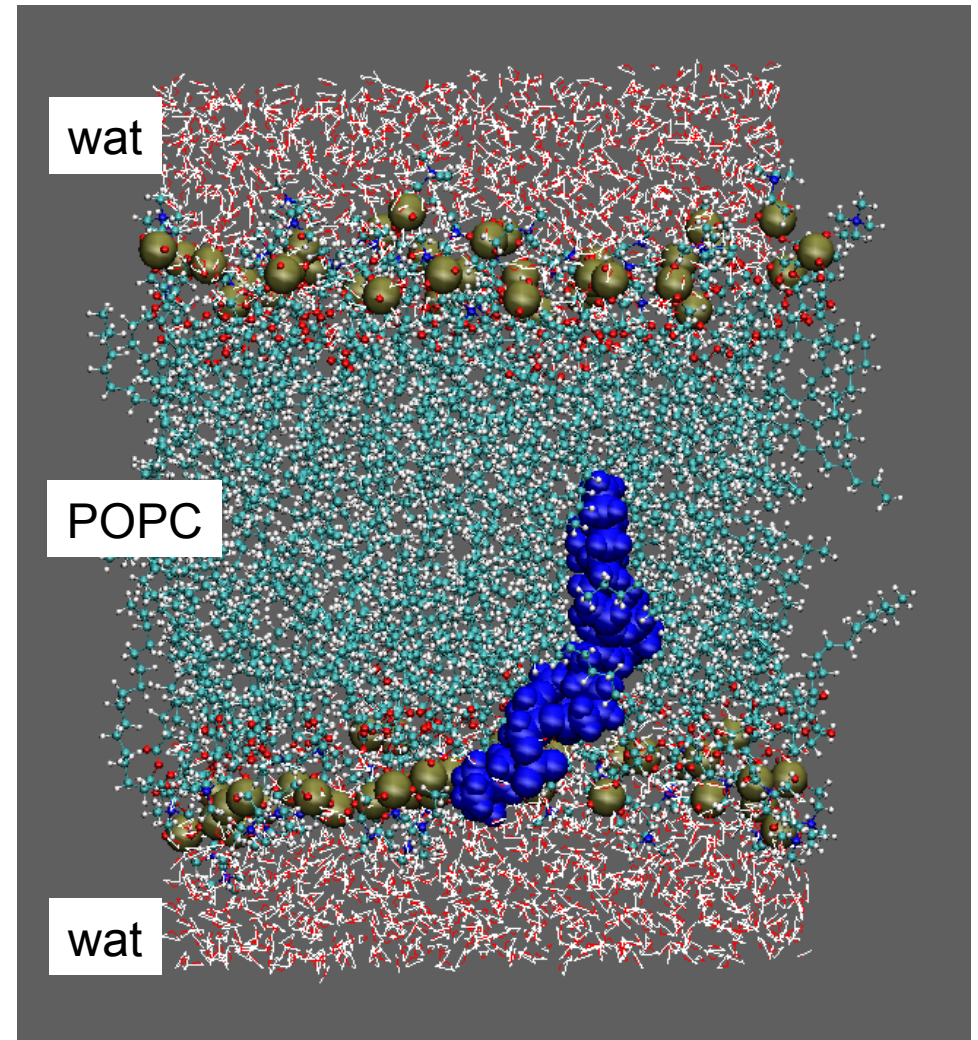
pure water

pure hexadecane

hexadecane layer  
in water

simple **POPC** bilayer  
containing only one lipid type

inner mitochondrial membrane: **MITO**  
modeled as bilayer with four lipid types



## Simulation details

CHARMM 36 force field

MD with CHARMM program

coupled (Nosé-Hoover) to thermostat (constant  $T$ ) and barostat (constant  $P$ )

**10** oxygen molecules are inserted  
(no quadrupole moment)

**box:** periodic boundary conditions (PBC)

width about 50 Angstrom in  $x,y$  direction

height between 52 and 70 Angstrom in  $z$  direction

POPC and MITO bilayer: 36 lipids on each side (72 total)

water layer is about 30 Angstrom thick

**initial run:** NPAT or NPT relaxation

$a = b$ , but  $c$  fluctuates independently

$T = 310$  K: body temperature

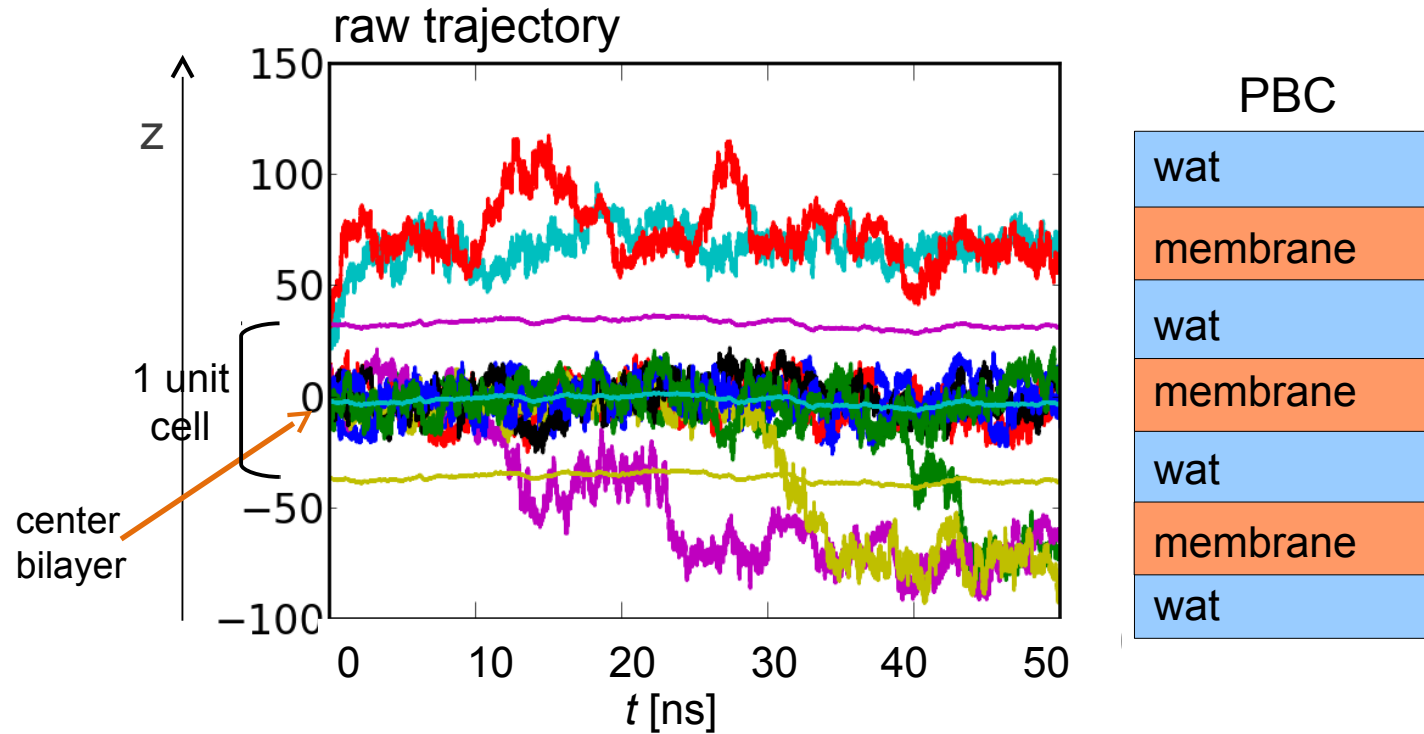
**production run:** NVT

time integration step 1 fs

sampling coordinates every 1 ps

50 ns for pure systems, 200 ns for layered systems

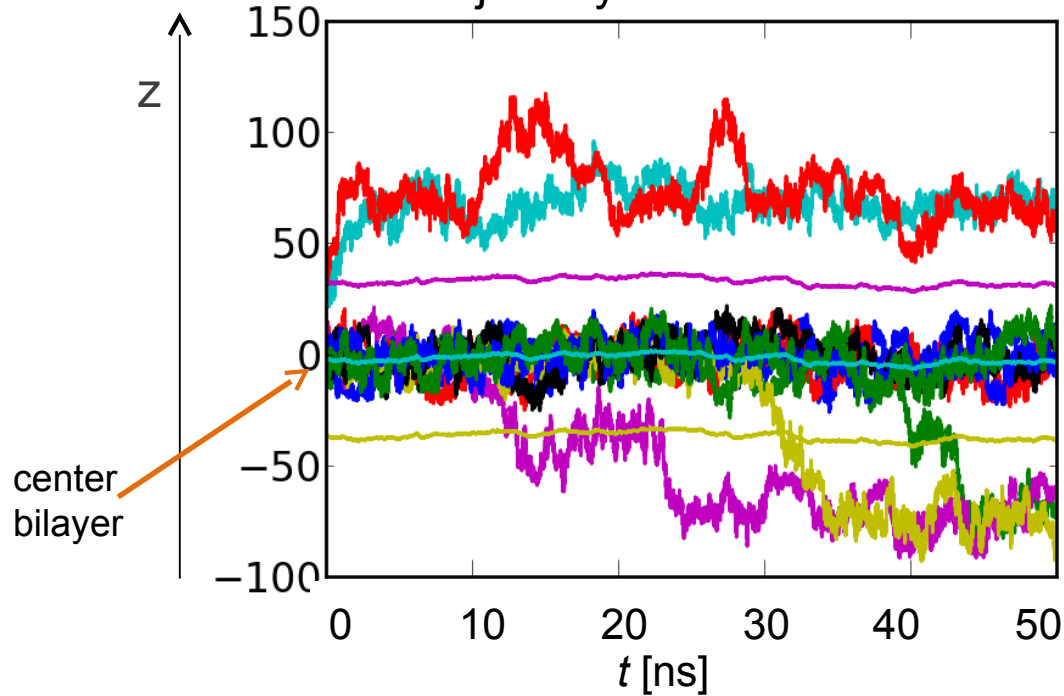
## Example: MITO



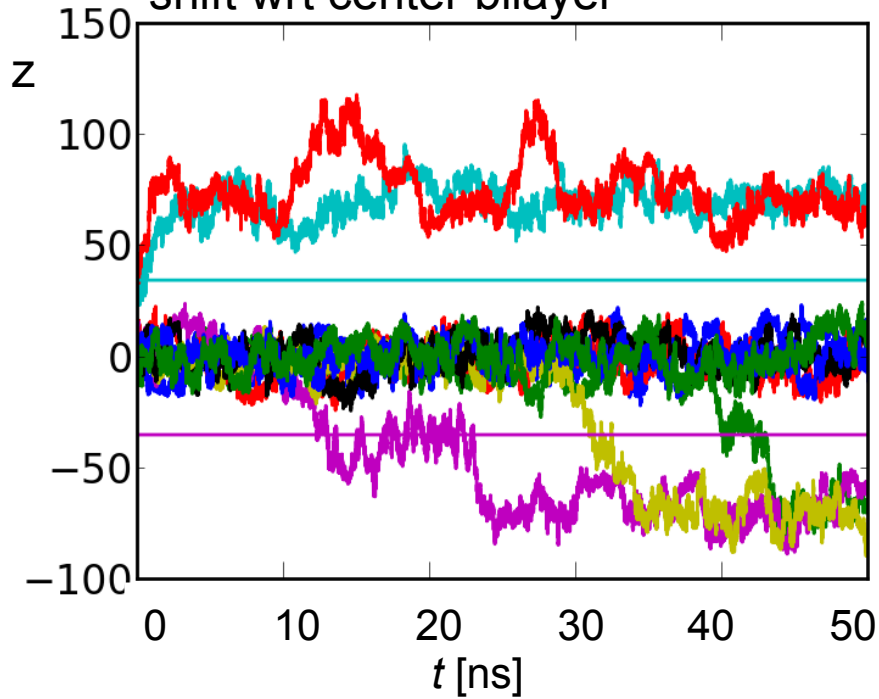
Define reaction coordinate: center of bilayer  
=> trajectories should be corrected for small drift

# Example: MITO

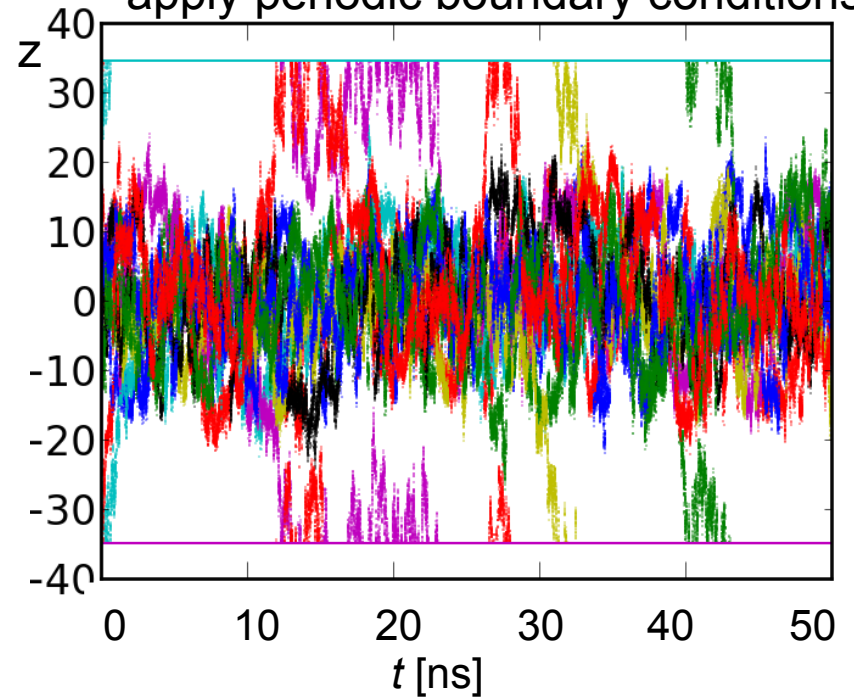
raw trajectory



shift wrt center bilayer



apply periodic boundary conditions



## Solving the diffusion equation in a layered medium

**general** 
$$\frac{\partial p(\bar{r}, t)}{\partial t} = \nabla \cdot \left[ \bar{\bar{D}}(\bar{r}) e^{-\beta F(\bar{r})} \nabla \left( e^{\beta F(\bar{r})} p(\bar{r}, t) \right) \right]$$

**translational symmetry** in the x,y-plane simplifies

free energy  $F(\bar{r}) \rightarrow F(z)$

diffusion tensor  $\bar{\bar{D}}(\bar{r}) \rightarrow \bar{\bar{D}}(z) = \begin{pmatrix} D_{||}(z) & 0 & 0 \\ 0 & D_{||}(z) & 0 \\ 0 & 0 & D_{\perp}(z) \end{pmatrix}$

## Solving the diffusion equation in a layered medium

**general** 
$$\frac{\partial p(\bar{r}, t)}{\partial t} = \nabla \cdot \left[ \bar{D}(\bar{r}) e^{-\beta F(\bar{r})} \nabla \left( e^{\beta F(\bar{r})} p(\bar{r}, t) \right) \right]$$

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using **polar coordinates**  $z$  and  $r = \sqrt{x^2 + y^2}$   
and initial conditions  $p(z, r, 0) = \delta(z - z_0) \delta(r)$   $p(\bar{r}, t) \rightarrow p(z, r, t) \rightarrow p(r, z, t | z_0)$

using **separation of variables**  $r$  and  $(z, t)$  **separation constant  $\alpha$**

(1) radial solution (textbook): Bessel functions of first type, zeroth order  $J_0(\alpha r)$

(2) orthogonal solution: functions  $Z_{\alpha}(z, t | z_0)$

=> the propagator: 
$$p(z, r, t | z_0) = \int d\alpha r J_0(\alpha r) Z_{\alpha}(z, t | z_0)$$

## Solving the diffusion equation in a layered medium

propagator  $p(z, r, t|z_0) = \int d\alpha r J_0(\alpha r) Z_\alpha(z, t|z_0)$

**Methodology: search for  $F, D$  profiles such that the propagator corresponds to the propagation observed in simulated trajectories**

$F, D$  profiles appear in the **derived propagators Q and Z**  
so do in two steps

## Solving the diffusion equation in a layered medium

propagator  $p(z, r, t|z_0) = \int d\alpha r J_0(\alpha r) Z_\alpha(z, t|z_0)$

**Methodology: search for  $F, D$  profiles such that the propagator corresponds to the propagation observed in simulated trajectories**

$F, D$  profiles appear in the **derived propagators  $Q$  and  $Z$**

(1)  $Q$  depends on  $F(z), D_\perp(z)$

$$Q(z, t) = \int p(z, r, t) dr$$

propagation from  
plane to plane in  
z-direction

$$\frac{\partial Q(z, t)}{\partial t} = \frac{\partial}{\partial z} \left[ D_\perp(z) e^{-\beta F(z)} \frac{\partial}{\partial z} \left( e^{\beta F(z)} Q(z, t) \right) \right]$$

$$Q(z, 0) = \delta(z - z_0) \rightarrow Q(z, t|z_0)$$

(2) set of  $Z$  depends also on  $D_\parallel(z)$

particles diffuse also radially

$$\frac{\partial Z_\alpha(z, t)}{\partial t} = \frac{\partial}{\partial z} \left[ D_\perp(z) e^{-\beta F(z)} \frac{\partial}{\partial z} \left( e^{\beta F(z)} Z_\alpha(z, t) \right) \right] - \alpha^2 D_\parallel(z) Z_\alpha(z, t)$$

sink term

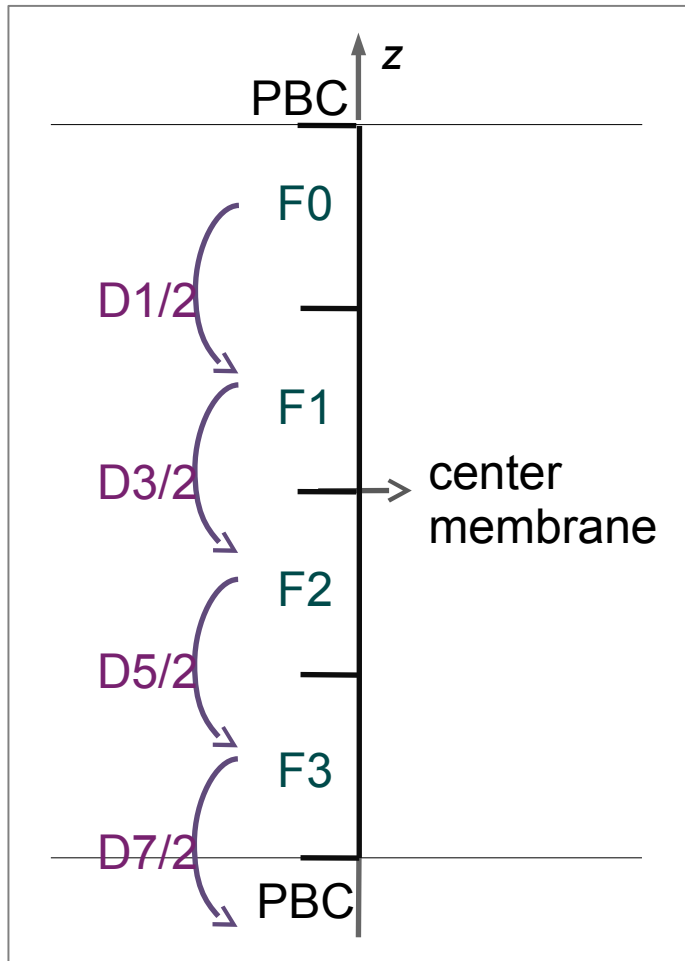
$$Z_\alpha(z, 0) = \alpha \delta(z - z_0) \rightarrow Z_\alpha(z, t|z_0)$$

# Calculating the diffusion profile with Monte Carlo

Solving 1-D equation: **binning the z-axis**

discretized profiles  $F_i$  and  $D_{i+1/2}$

PBC: periodic boundary conditions

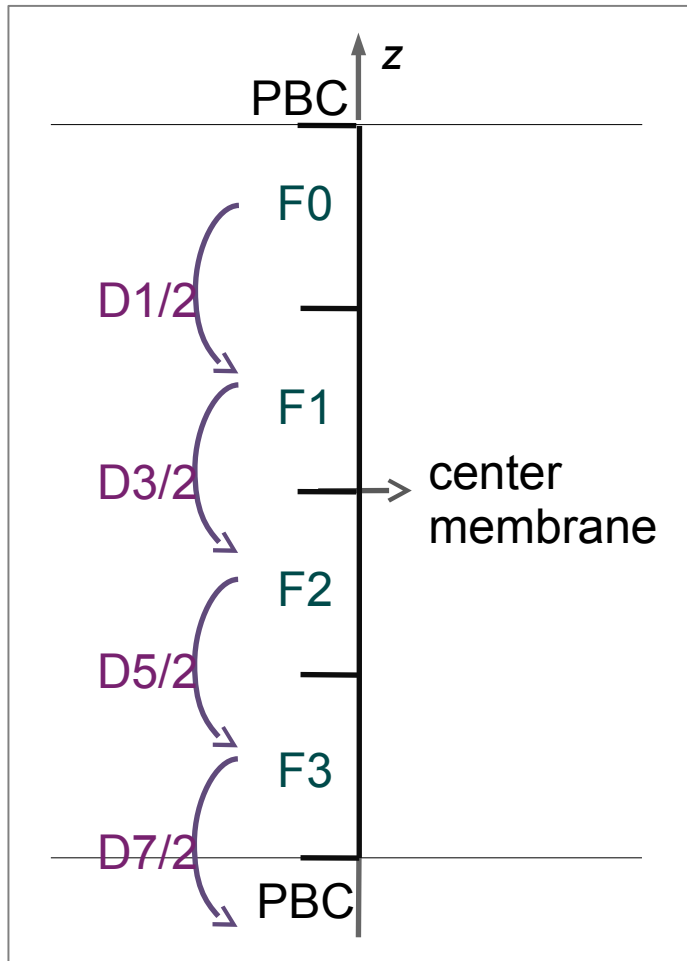


# Calculating the diffusion profile with Monte Carlo

Solving 1-D equation: **binning the z-axis**

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$$\frac{\partial Q(z,t)}{\partial t} = \frac{\partial}{\partial z} \left[ D_{\perp}(z) e^{-\beta F(z)} \frac{\partial}{\partial z} \left( e^{\beta F(z)} Q(z,t) \right) \right]$$

rate equations: discretized  $Q(z,t)$  equation

$$\dot{Q}_i(t) = \sum_j R_{ij} Q_j(t)$$

$Q_i$  is probability to be in bin  $i$

with rate matrix  $R$ , e.g.

$$R_{i+1,i} = D_{i+1/2} \exp[-\beta(F_{i+1} - F_i)]$$

given start bin  $j$   
what is probability to be in bin  $i$   
after a lag time  $t$ ?

$$P(i,t|j) = [\exp(tR)]_{ij}$$

matrix exponential

**discretized propagator**

## Calculating the diffusion profile with Monte Carlo

We want to determine the profile  $F(z)$ ,  $D_{\perp}(z)$ ,  $D_{\parallel}(z)$

This is done by comparing TRAJECTORIES (T) with the diffusion MODEL (M).

### TRAJECTORIES (T)

from computer experiment  
molecular dynamics



### MODEL (M)

$F(z)$ ,  $D_{\perp}(z)$ ,  $D_{\parallel}(z)$

The optimal model **M** has the maximum likelihood.

**likelihood = L = P(T|M)**

= probability that model **M** explains/produces available data **T**

Model parameters should be varied, until the model is found that is most likely to produce the measured trajectories.

We want to find the maximum of the P(T|M) distribution.

=> **maximum-likelihood method**

Alternatively, the whole P(T|M) distribution is sampled, by testing all possible models.

=> **Bayesian analysis**

# Calculating the diffusion profile with Monte Carlo

## TRAJECTORIES (T)

molecular dynamics

$$z(t)$$

↓ discretize

$$i(t)$$



## MODEL (M)

$$F(z), D_{\perp}(z)$$

↓ discretize

$$F_i, D_{\perp, i+1/2}$$

**count** transitions

from bin  $j$  to bin  $i$

when waiting for some time  $t$

( $t = \text{lag time}$ )

construct rate matrix  $R$

histogram  $N_{ij}(t)$

propagator  $P(i, t|j) = [\exp(tR)]_{ij}$

**likelihood**

$$L \sim P(T|M) = \prod_{\substack{\text{trans} \\ j \rightarrow i}} [\exp(tR)]_{ij}^{N_{ij}}$$

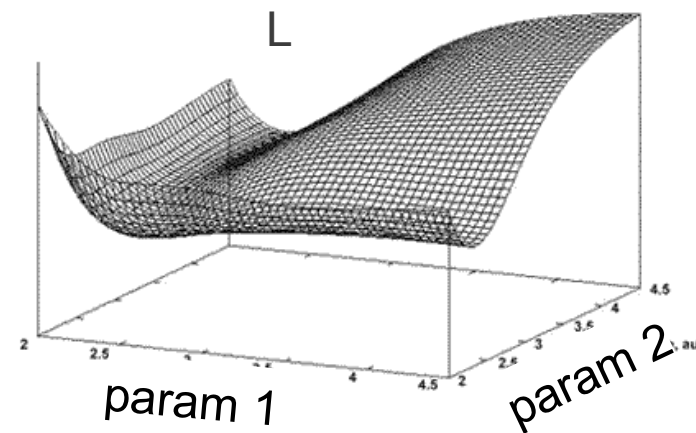
$$\ln L \sim \ln P(T|M) = \sum_{\substack{\text{trans} \\ j \rightarrow i}} N_{ij} \ln [\exp(tR)]_{ij}$$

in practice: use  $\ln(L)$

# Calculating the diffusion profile with Monte Carlo

$$\text{likelihood} = L = P(T|M)$$

regard  $L$  as a surface in model parameter space  
and use Monte Carlo to construct surface  
in practice:  $\ln(L)$  surface



## Monte Carlo (MC) algorithm

- propose new parameters
- calculate  $L$
- compare old  $L$  and new  $L$ 
  - if  $L$  increases: accept new
  - if  $L$  decreases: accept new with probability

$$e^{\frac{\ln L_{\text{new}} - \ln L_{\text{old}}}{T}}$$

$T$  is parameter temperature

- => Maximum  $L$ : reduce parameter temperature gradually to “freeze” to a local extremum.
- => Bayesian analysis:  $T=1$

# Calculating the diffusion profile with Monte Carlo

## Extension to 2-D

in practice, **apply a boundary condition**: far away, concentration is zero  
=> condition  $p(r=s)=0$  discretizes  $\alpha$

$$p(z, r, t|z_0) = \sum_{\alpha_k s=x_k} r J_0(\alpha_k r) Z_{\alpha_k}(z, t|z_0)$$

$x_k$  zeros of Bessels

remember 1-D  $\dot{Q}_i(t) = \sum_j R_{ij} Q_j(t)$

sink term

now we have  $\dot{Z}_{\alpha,i}(t) = \sum_j (R_{ij} - \alpha^2 D_{||,i} \delta_{ij}) Z_{\alpha,j}(t)$

given start bin  $j$

what is probability to be in z-bin  $i$  and r-bin  $m$

after a lag time  $t$ ?

$$P(i, m, t|j) = \sum_{\alpha_k s=x_k} r_m \frac{J_0(\alpha_k r_m)}{\pi J_1^2(\alpha_k s)} \left[ \exp(tR - t\alpha_k^2 \mathcal{D}_{||}) \right]_{ij}$$

sink term

sum over Bessels

**discretized propagator**

# Calculating the diffusion profile with Monte Carlo

## Extension to 2-D

### TRAJECTORIES (T)

molecular dynamics

$$x(t), y(t), z(t)$$

↓ discretize z-bins, r-bins

$$i(t), m(t)$$



### MODEL (M)

$$F(z), D_{\perp}(z), D_{\parallel}(z)$$

↓ discretize

$$F_i, D_{\perp, i+1/2}, D_{\parallel, i}$$

### count transitions

from z-bin  $j$  to z-bin  $i$  and r-bin  $m$

when waiting for some time  $t$

( $t = \text{lag time}$ )

histogram  $N_{im,j}(t)$

construct rate matrix  $R$

and sink term

propagator  $P(i, m, t|j)$

### likelihood

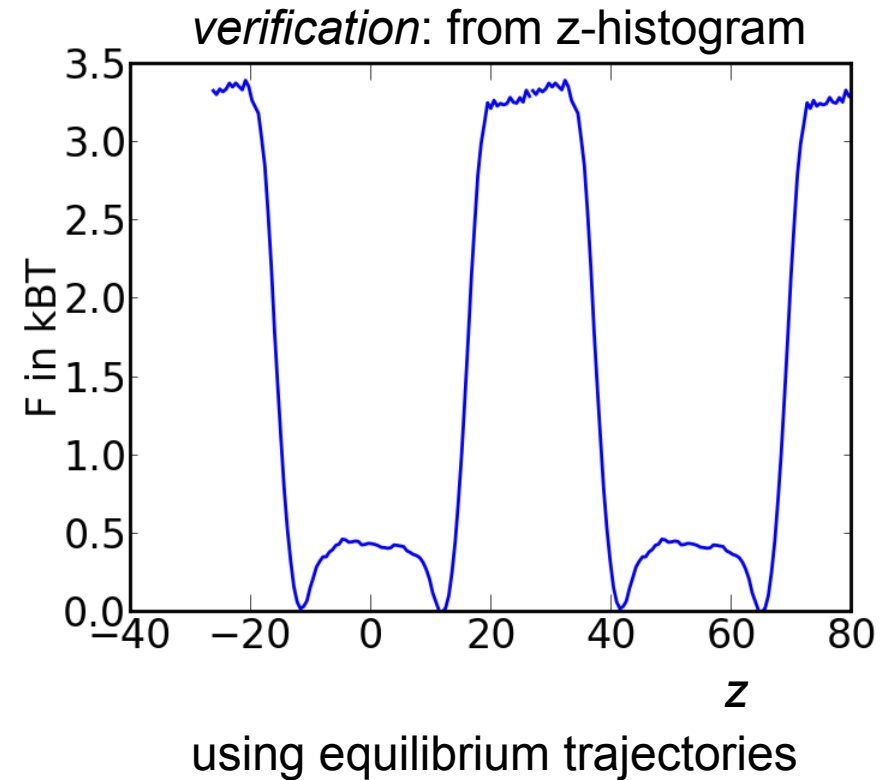
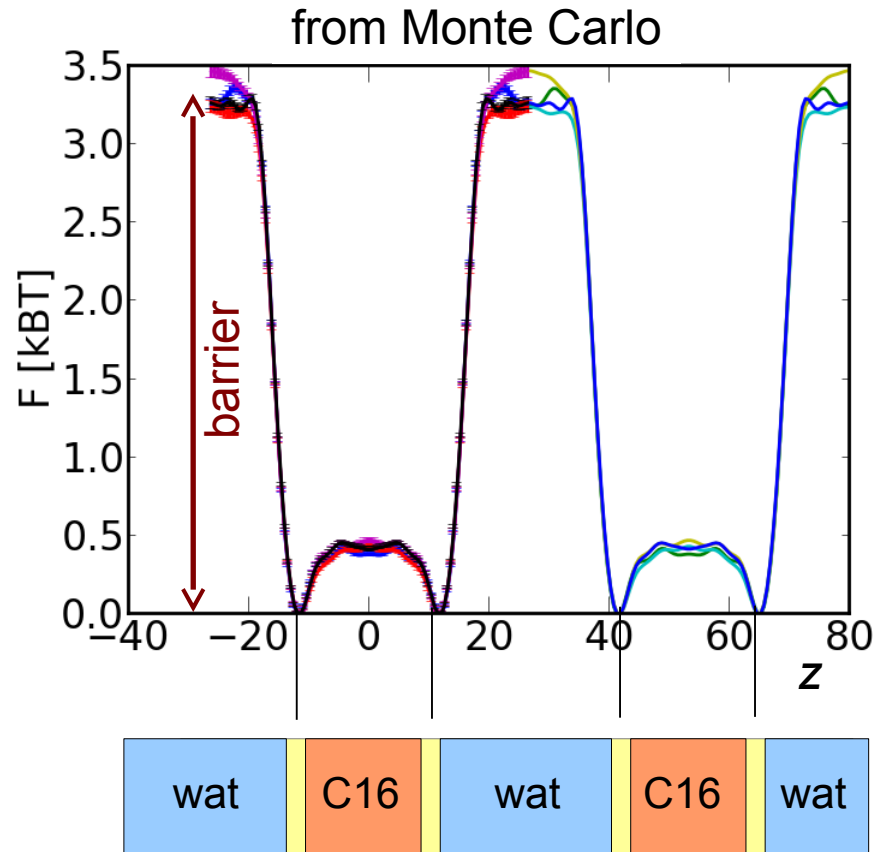
$$\ln L = \sum_{\substack{\text{trans} \\ j \rightarrow i, m}} N_{im,j} \ln [P(i, m, t|j)]$$

## Outline – Simulating oxygen diffusion through membranes

1. Diffusion in inhomogeneous and anisotropic media
2. Five test systems:
  - pure water, pure hexadecane, hexadecane layer in water
  - simple POPC bilayer
  - model for inner mitochondrial membrane
3. Deriving diffusion profiles from statistics
4. Free energy profiles and diffusion profiles

# Free energy profile $F(z)$ for oxygen in C16-layer/water

potential of mean force felt by  $O_2$  molecule



barrier:  $3.4 k_B T$

preferential location: at interface C16/wat (grooves) or in C16

# Free energy profile $F(z)$ for oxygen in membranes

Improvements Monte Carlo routine:

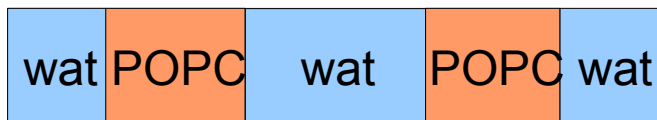
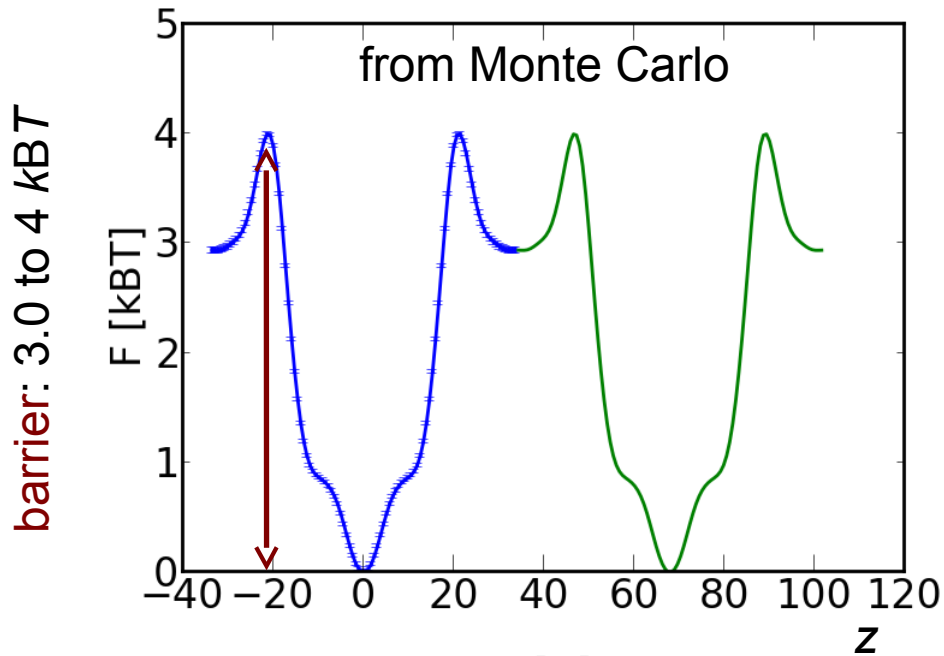
1) to improve smoothness:  
add penalty function  $\sum_i (f_i - f_{i+1})^2$

$$F(z) = \sum_n a_n \cos(\omega_n z)$$

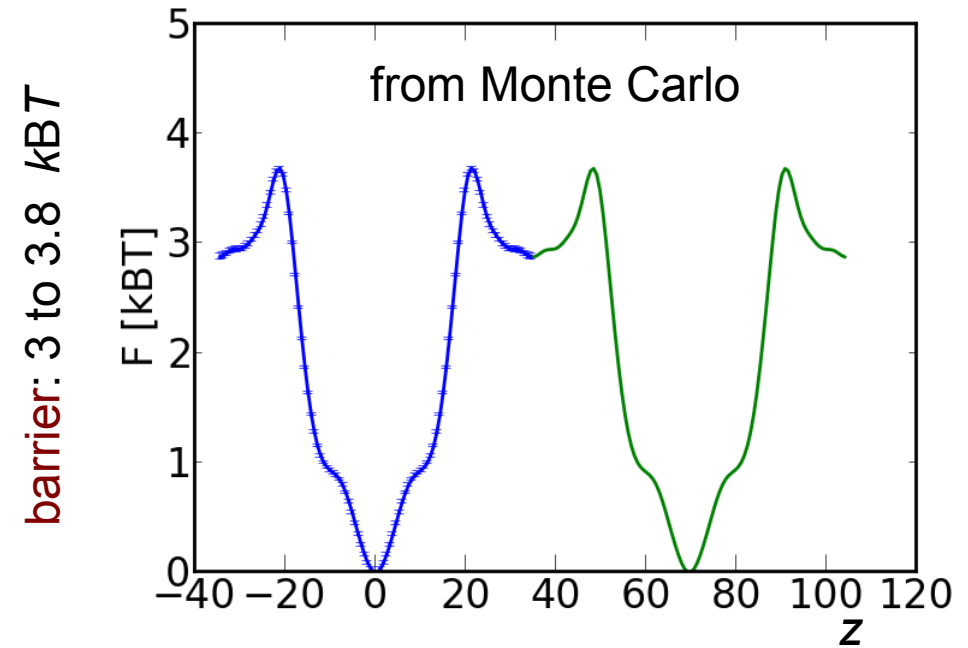
2) to impose symmetry, improve smoothness:  
express  $F$  and  $D$  with basis functions

$$\ln D(z) = \sum_n b_n \cos(\omega_n z)$$

## POPC



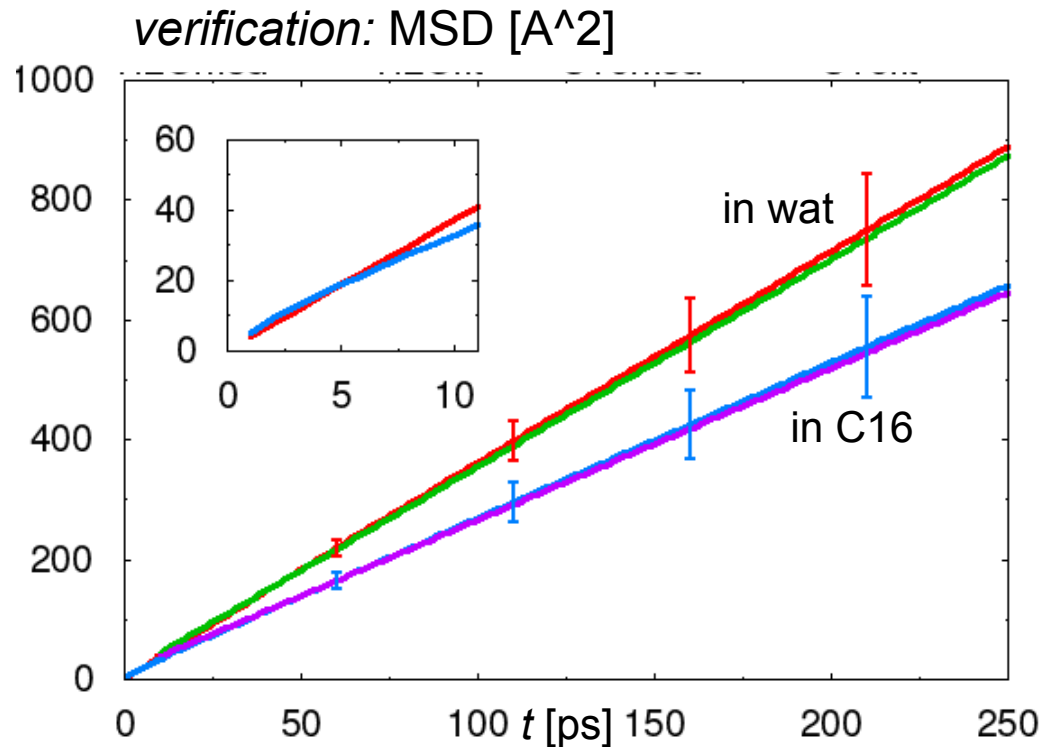
## MITO



# Oxygen diffusion $D_{\perp}(z)$ : validation in pure phase

	$t = 1$ ps	$t = 10$ ps	$t = 100$ ps
pure wat			
from Monte Carlo	0.83	0.64	0.61
from MSD	0.85	0.63	0.60
pure C16			
from Monte Carlo	1.02	0.56	0.45
from MSD	1.03	0.56	0.46

all  $D$  values in  $\text{\AA}^2/\text{ps}$   
 error:  $\pm 0.02 \text{\AA}^2/\text{ps}$



**for bulk  $D$  (where  $F$  is flat):  
 Monte Carlo corresponds to MSD**

*Note on lag times:*  
 choose  $t > 5$  ps  
 to see long time behavior

# Inner mitochondrial membrane composition

Three dominant head groups: PE, PC, CL

<i>head</i>	<i>%P</i>	<i>%lipid</i>
PE	37.9	49
PC	26.5	34
CL	25.4	16

are combined with saturated/unsaturated tails

	PE	PC	CL
14-0	1.7	2.4	1.4
15-0	1.8	5.6	0.0
16-0	9.1	27.6	9.0
17-0	2.0	0.8	1.6
18-0	19.7	9.4	6.3
16-br	3.2	1.0	1.7
18-br	2.6	1.0	0.0
16-1	3.8	1.6	2.4
18-1	8.6	16.4	11.5
18-2	22.1	29.0	65.2
18-3	2.3	1.3	0.0
20-1	2.1	0.0	0.0
20-4	20.5	1.8	0.0
% saturated	39.1	47.8	20.0
% unsaturated	59.4	52.1	79.1
ratio	66%	91%	25%

composition in simulations:

<i>name</i>		<i>head</i>	<i>sn1</i>	<i>sn2</i>	<i>sn3</i>	<i>sn4</i>
SAPE	9/side	PE	18-0	20-4		
SLPE	9/side	PE	18-0	18-2		
PLPC	12/side	PC	16-0	18-2		
CL	6/side	CL	16-0	18-2	18-2	18-2

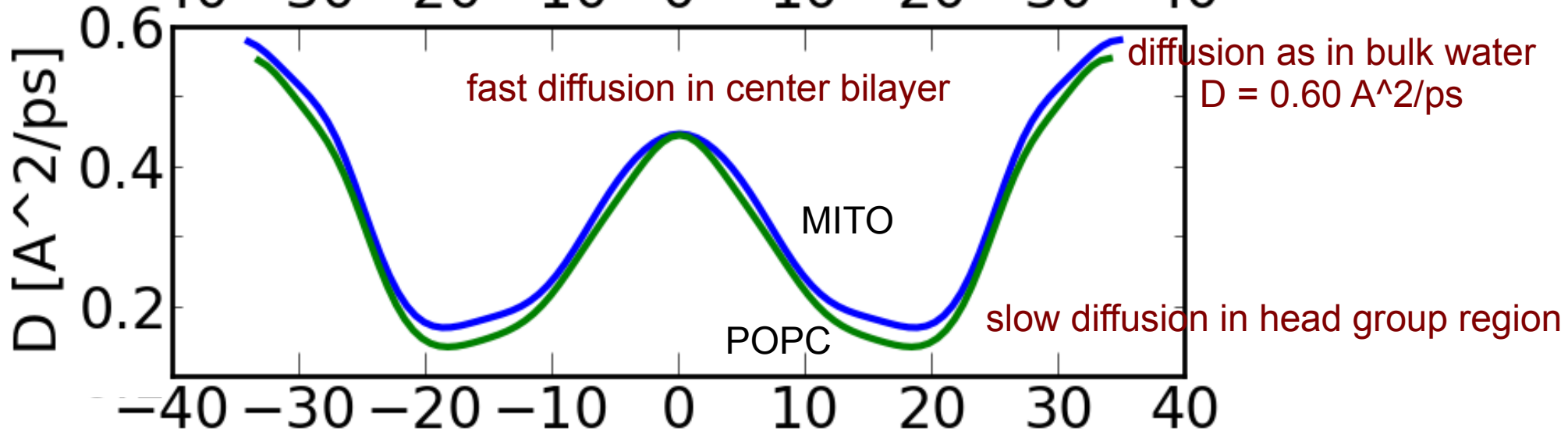
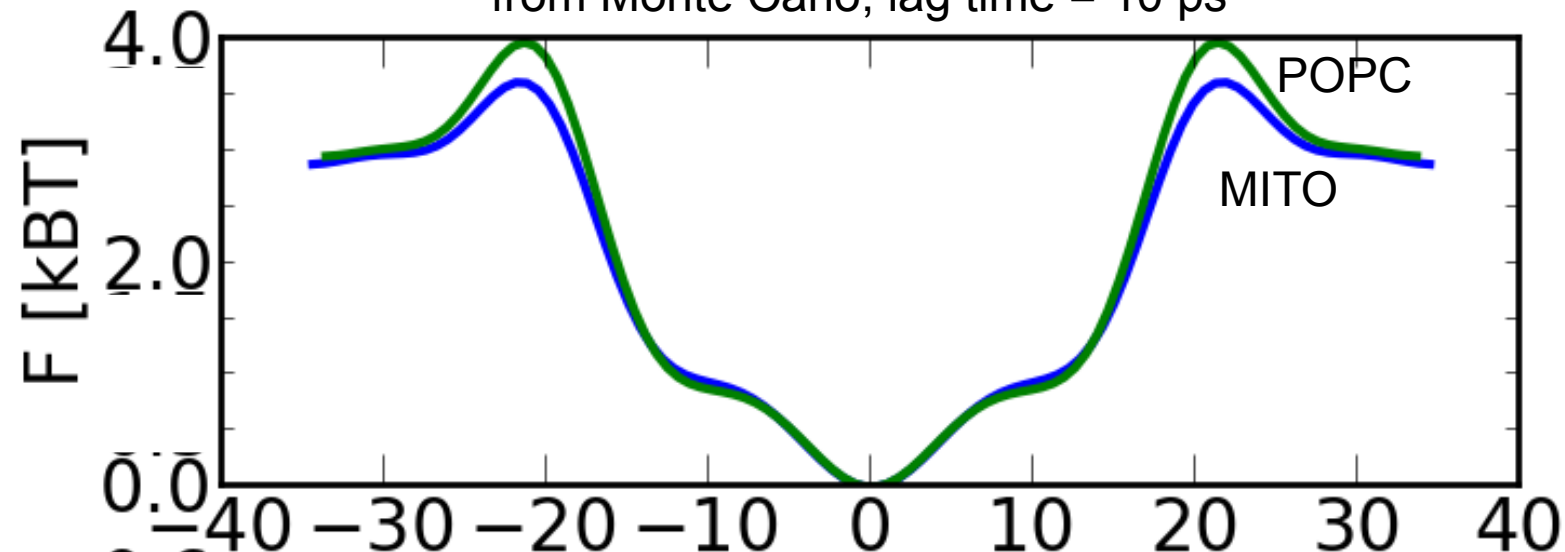
Comte, Maisterrena, Gautheron  
 Biochim. Biophys. Acta 419, 271-284 (1976)

and not yet speaking about plasmalogens, cholesterol, lipids, etc...

# Oxygen diffusion $D_1(z)$ in membranes

little difference between  
POPC and MITO

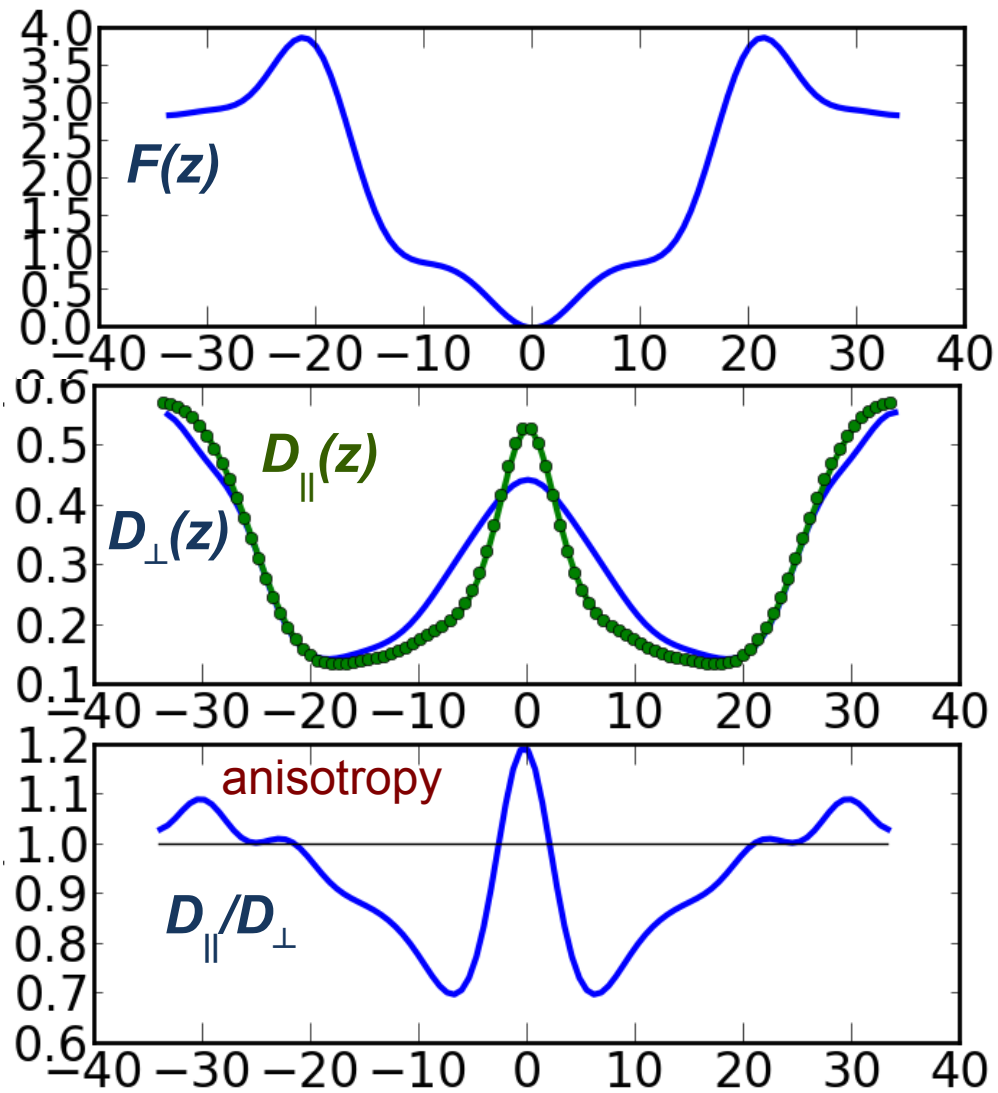
from Monte Carlo, lag time = 10 ps



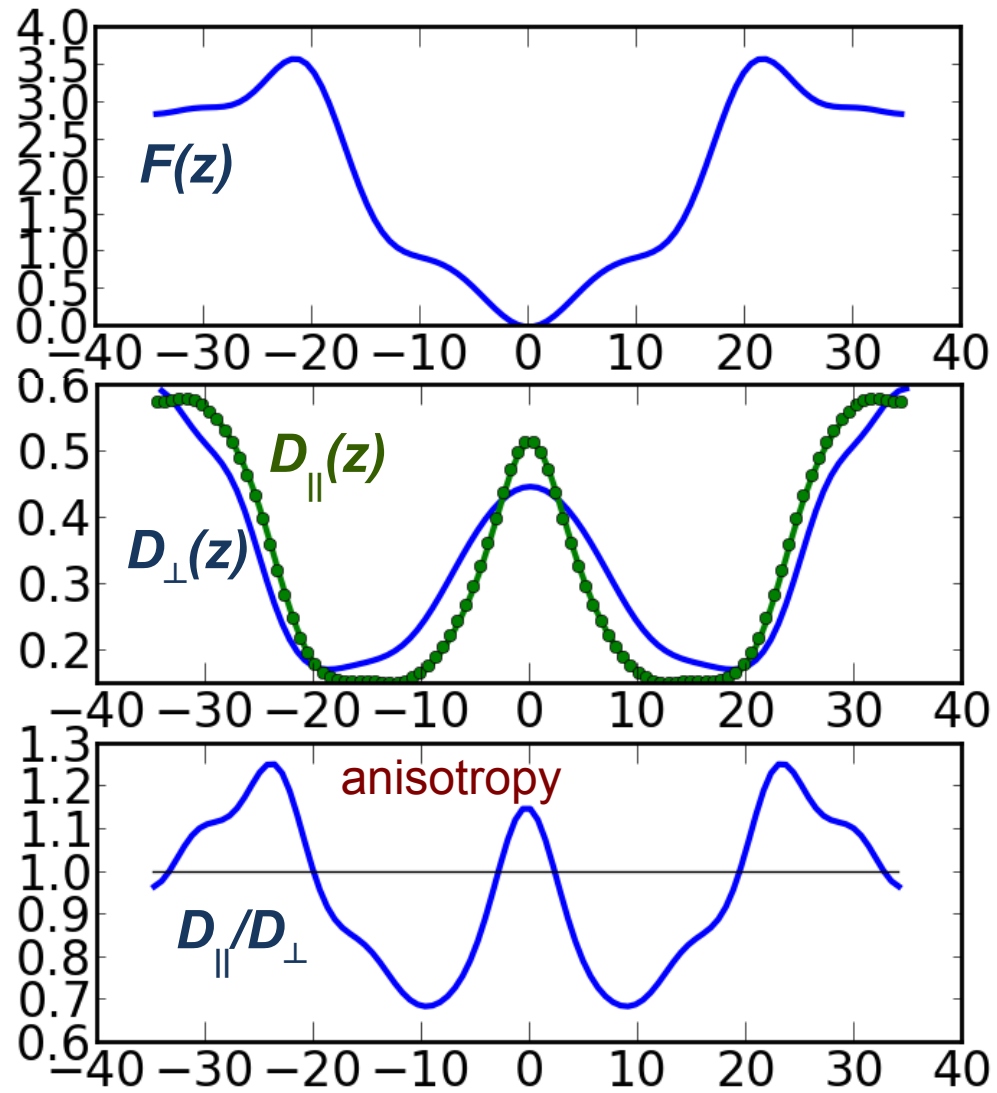
# Oxygen diffusion $D_{\parallel}(z)$ in membranes

little difference between  
POPC and MITO

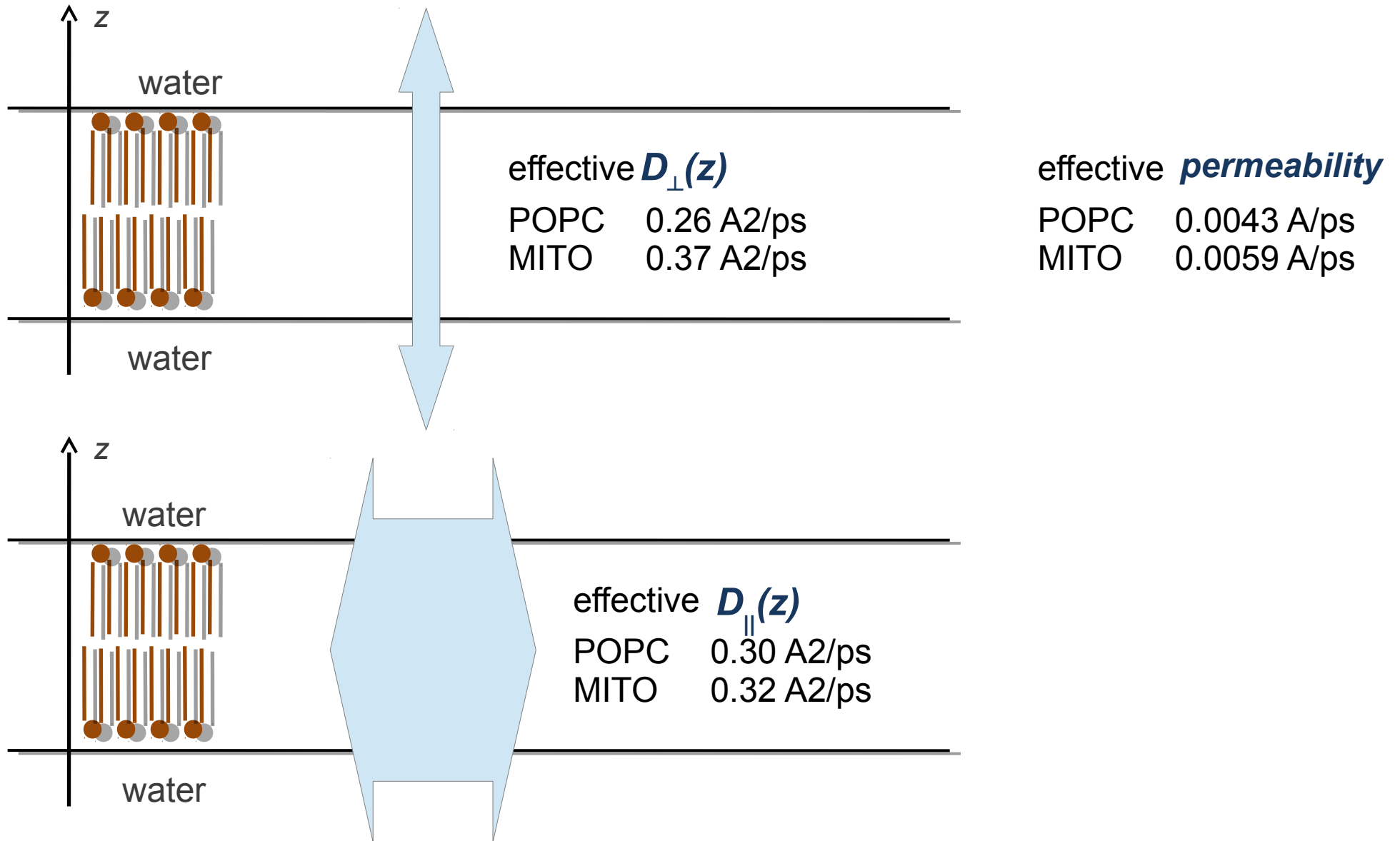
## POPC



## MITO



## Efficiency of oxygen diffusion: fluxes



1. Membranes capture oxygen (slower than in bulk water  $D = 0.58 \text{ A}^2/\text{ps}$ )
2. Diffusion in MITO is approx 30% more efficient

# Conclusions

## 1. Methodology:

Membranes are inhomogeneous and anisotropic.

The standard MSD-versus-time method then requires short lag times.

We constructed profiles using Bayesian analysis (Monte Carlo), allowing for longer lag times.

## 2. Profiles

Head-group region: diffusion is slow, free energy barrier

Center of bilayer: diffusion is fast, free energy is favorable

## 3. Anisotropy

Tail region: faster along the direction of the chains, than in radial direction

Center of bilayer: radially faster than in orthogonal direction.

## 4. Efficiency

Membranes capture oxygen (slower diffusion than in bulk water).

Little difference in POPC and MITO profiles.

Nevertheless, diffusion in MITO is approx 30% more efficient than in POPC.

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National Heart Lung Blood Institute

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